



IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

APPLICATION FOR UNITED STATES PATENT

FOR

**APPARATUS FOR REDUCING  
FLUID DRAWBACK THROUGH A MEDICAL VALVE**

Inventors:

**Andrew L. Cote, Sr.**  
1 Linden Way  
Merrimack, NH 03054

**Brian L. Newton**  
34 Foster Street  
Woonsocket, RI 02895

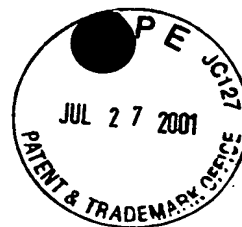
**Charles F. Ganem**  
1 Key Way  
Cape Neddick, Maine 03902

Attorney Docket: 1600/138

Attorneys:

**BROMBERG & SUNSTEIN LLP**  
125 Summer Street  
Boston, MA 02110  
(617) 443-9292

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## **APPARATUS FOR REDUCING FLUID DRAWBACK THROUGH A MEDICAL VALVE**

### **PRIORITY**

This patent application claims priority from U.S. patent application number 09/479,327, filed January 6, 2000 (attorney docket number 1600/121). As a consequence of this priority claim, this application also claims priority to U.S. provisional patent application serial number 60/117,359, filed January 27, 1999.

### **FIELD OF THE INVENTION**

The invention generally relates to medical products and, more particularly, the invention relates to devices for reducing backflow through a medical valve.

### **BACKGROUND OF THE INVENTION**

Medical valving devices commonly are utilized to valve fluids injected into and withdrawn from a patient. One exemplary type of medical valving device, known in the art as a "catheter introducer," maintains a sealed port for accessing the patient's vasculature. Use of such a valve enables vascular access without requiring the patient's skin to be repeatedly pierced by a needle. Moreover, catheter introducers are constructed to withstand a range of back-pressures produced by a patient's blood pressure, thus minimizing blood loss resulting from fluid injections or withdrawals.

Fluid commonly is transferred to/from a patient by inserting a syringe (*e.g.*, a needle) into a medical valve, thus communicating with the patient's vasculature. Problems arise, however, when the syringe is withdrawn from the valve. More particularly, a back pressure produced by withdrawing the syringe undesirably can cause blood to leak proximally into various parts of the valve. In addition to coagulating and impeding the mechanical operation of the valve, blood in the valve also compromises the sterility of the valve.

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## SUMMARY OF THE INVENTION

In accordance with one aspect of the invention, a medical valve for valving fluid includes a housing defining a chamber having an inlet, an outlet, and an interior wall, a compressible member within the chamber, and a fluid channel defined by the interior wall. The fluid channel directs fluid received from the inlet toward the outlet.

In preferred embodiments, the compressible member does not occlude fluid flow through the fluid channel. The compressible member may be any compressible object that is made from any compressible material known in the art. For example, the compressible member may be made from a sponge material. The compressible member also may be made from a material that merely expands and contracts in response to a mechanical force. For example, the compressible member may be a balloon device. The medical valve also may include a plunger, having a distal end within the interior, that controls the volume of the variable volume interior.

In some embodiments, the valve is movable between open and closed positions. In such case, the compressible member may cooperate with the interior to cause the interior to have a greater available volume (for containing fluid) when the valve is open than when the valve is closed. Accordingly, as the valve closes (and the available volume decreases), residual fluid within the valve should be forced from the chamber toward the outlet of the valve.

In accord with another aspect of the invention, a medical valve having an open mode for permitting fluid flow through the valve, and a closed mode for preventing fluid flow through the valve, includes an interior wall defining a variable volume fluid chamber, and a compressible member within the variable volume fluid chamber. The compressible member and interior wall together define both a closed chamber volume within the fluid chamber when the valve is in the closed mode, and an open chamber volume when the valve is in the open mode. The closed chamber volume preferably is no greater than the open chamber volume, thus reducing the potential for fluid drawback that may result when transitioning from the open mode to the closed mode.

In preferred embodiments, the interior wall defines a channel for channeling fluid flow

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through the valve. The compressible member preferably does not occlude fluid flow through the valve since it does not occlude the channel.

In accord with other aspects of the invention, a medical valve for valving fluid permits fluid flow when in an open mode and prevents fluid flow when in a closed mode. The valve includes an interior wall defining a chamber, and a compressible member within the chamber. The compressible member has a maximum volume and a minimum volume. The compressible member has a volume that is equal to the maximum volume when the valve is in the closed mode. In a similar manner, the compressible member has a volume that is equal to the minimum volume when in the open mode.

In preferred embodiments, the minimum volume is smaller than the maximum volume. In addition, the interior wall defines a channel for channeling fluid through the valve when in the open mode. In other embodiments, the compressible member and chamber cooperate to define a closed chamber volume when the valve is in the closed mode, and an open chamber volume when the valve is in the open mode. The closed chamber volume preferably is greater than the open chamber volume.

In accordance with yet another aspect of the invention, a medical valve includes a housing defining both a valve chamber and a fluid passageway for directing fluid through the valve, a compressible member within the chamber, and a vent defined by a wall of the chamber (chamber wall) extending through the housing to vent the member chamber. In addition, the valve chamber has an inlet for receiving fluid from the fluid passageway. The compressible member divides the valve chamber into a fluid chamber and a member chamber, where the fluid chamber receives fluid through the inlet and has an outlet for directing fluid to the fluid passageway. The member chamber is defined by the compressible member and the chamber wall and thus, includes the vent.

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### BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing and other objects and advantages of the invention will be appreciated more fully from the following further description thereof with reference to the accompanying drawings wherein:

Figure 1 schematically shows a medical valve that may be constructed in accord with preferred embodiments of the invention.

Figure 2 schematically shows a cross-sectional view of a first illustrative embodiment of the medical valve shown in figure 1 along line 2-2.

Figures 3A-3D schematically show the cross-sectional view of the valve shown in figure 2 as it is urged from a closed mode to an open mode.

Figure 4 schematically shows a cross-sectional view of a second illustrative embodiment of the valve shown in figure 1.

Figure 5A shows a perspective view of a compressible member utilized with the second illustrative embodiment of the valve.

Figure 5B shows a perspective view of an end cap utilized with various embodiments of the valve.

Figure 5C shows a plan view of the end cap shown in figure 5B.

Figure 5D shows a cross-sectional view of the end cap shown along line A-A of figure 5C.

Figure 6 schematically shows a cross-sectional view of a third illustrative embodiment of the valve shown in figure 1.

Figure 7 schematically shows a cross-sectional view of a fourth illustrative embodiment of the valve shown in figure 1.

Figure 8 schematically shows a cross-sectional view of a fifth illustrative embodiment of the valve shown in figure 1.

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## DESCRIPTION OF PREFERRED EMBODIMENTS

Figure 1 schematically shows a medical valve 5 that preferably is configured to reduce fluid drawback (a/k/a "back-flow") when a syringe or other type of nozzle is withdrawn from it. Accordingly, the valve 5 includes a proximal fluid port 10 for receiving the nozzle, a valve body 11 having a valving mechanism (figures 2 and 3A-3D) that controls fluid flow through the valve 5, and a distally located fluid port 50 for directing fluid between the valve 5 and a patient. The fluid preferably is in liquid form, such as liquid medication. Although much of the discussion herein refers to the proximal port 10 as a fluid inlet, and the distal port 50 as a fluid outlet, the proximal and distal ports 10 and 50 also may be utilized respectively as outlet and inlet ports. In preferred embodiments, the valve 5 is similar to that disclosed in U.S. Patent Application No. 09/394,169, entitled, "SWABBABLE LUER-ACTIVATED VALVE," filed September 13, 1999 and naming Andrew Cote and Charles Ganem as inventors, the disclosure of which is incorporated herein, in its entirety, by reference. It should be noted that although preferred embodiments are discussed with reference to the above noted patent application, principles of the invention may be applied to other medical valve devices having dissimilar structures to those medical valves shown. As discussed below, the distal port 50 of the valve 5 may be at its location shown in figure 1, or at a location that is orthogonal to the longitudinal dimension of the valve 5.

Figure 2 schematically shows a cross-sectional view of a first embodiment of the medical valve 5 shown in figure 1 along line 2-2. Among other things, the valve 5 includes an inlet housing portion 34 having the proximal port 10, an outlet housing portion 48 having the distal port 50, a stretchable and compressible gland 12 secured between the inlet housing 34 and outlet housing 48, and a rigid, longitudinally movable cannula 14 secured within the valve 5 by the gland 12. The cannula 14 forms a cannula flow channel 36 terminating at a transverse channel 28 that normally is occluded by the gland 12. In addition, the outlet housing 48 forms a chamber 65 having a volume that changes as the cannula 14 is urged proximally and distally by a nozzle.

Insertion of a nozzle against a slit 42 at the proximal end of the gland 12 causes the cannula 14 to move distally, thereby moving the transverse channel 28 from its occluding contact

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with the gland 12. Liquid then may be directed first through the cannula channel 36 and transverse channel 28, then through the variable volume chamber 65, and out of the valve 5 through the distal port 50. Details of the cooperation of the various valving mechanisms within the valve 5 are more fully described in the aforementioned co-pending U.S. patent application.

In accord with preferred embodiments of the invention, the valve 5 also includes a compressible member 41 positioned within the chamber 65, and one or more narrow flow channels formed in the interior wall forming the chamber 65. One exemplary narrow flow channel is shown in phantom at reference number 43. The compressible member 41 cooperates with the cannula 14 to reduce the available volume within the chamber 65 that may be utilized to contain fluid within the valve 5. In preferred embodiments, the compressible member 41 occupies substantially the entire volume of the chamber 65 when the valve 5 is closed (*i.e.*, in a "closed mode").

The narrow flow channels 43 are not occluded by the compressible member 41 and thus, are utilized to direct fluid around the compressible member 41 and toward the distal port 50. In preferred embodiments, the narrow flow channels 43 are in the form of relatively deep and narrow grooves formed in the interior walls of the distal housing 48. It is anticipated that flow channels 43 having a depth of about 0.040 - 0.060 inches, and a width of about 0.020 - 0.040 inches would produce satisfactory results. These dimensions are not exact, however, and may be modified as necessary. Accordingly, practice of the invention should not be limited to these preferred dimensions. In preferred embodiments, the valve 5 includes three independent grooves longitudinally spaced about 120 degrees apart across the cylindrical inner surface of the variable volume chamber 65.

The compressible member 41 may be any apparatus that performs the dual function of compressing and expanding within the chamber 65, and limiting available chamber volume for containing liquid. Accordingly, such a member 41 directs liquid to the narrow channels 43, thus bypassing the chamber 65. In preferred embodiments, the compressible member 41 is a medical grade closed cell sponge rubber that is produced by conventional injection molding processes. Such member 41 may be made by injecting an elastomeric material with a nitrogen gas, and

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surrounding the injected elastomer with an outside skin, such as rubber. As shown in the figures, the compressible member 41 of this embodiment occupies most of the volume of the chamber 65 at all times (*i.e.*, between the times when the valve 5 is opened, and when the valve 5 is closed).

In alternative embodiments, the compressible member 41 is a latex or polyester balloon having a hollow interior. The balloon changes shape based upon the position of the cannula 14. Regardless of the type of apparatus is used as the compressible member 41, however, its use necessarily adds a degree of mechanical resistance to the longitudinal movement of the cannula 14.

Figures 3A-3D schematically show the cross-sectional view of the valve 5 shown in figure 2 as it is urged from a closed mode to an open mode. More particularly, figure 3A shows the valve 5 as a nozzle is about to be inserted through the proximal port 10. Figures 3B-3D show the nozzle at various stages of progression through the proximal port 10 and into the inlet housing 34. More particularly, as shown in figure 3A, the compressible member 41 occupies substantially all of the chamber volume when the valve 5 is in the closed mode. As the nozzle is inserted, however, the compressible member 41 compresses between the (distally moving) distal end of the cannula 14 (that acts as a plunger) and the distal end of the interior wall of the chamber 65. As the compressible member 41 compresses (*i.e.*, thereby having a decreasing volume), a proximal region of the chamber 65 (hereinafter "proximal chamber 66") begins to form and increase in size until the valve 5 is in the fully open mode (figure 3D). When the valve 5 is in the fully open position, the compressible member 41 is compressed to a minimum volume within a distal portion of the chamber 65 (hereinafter "distal chamber 67"). In some embodiments, the proximal chamber 66 has a volume that is about equal to or less than that of the distal chamber 67.

The total available volume for containing liquid in the chamber 65 preferably is greater when the valve 5 is open than when the valve 5 is closed. Accordingly, when in the open mode (figure 3D), liquid can collect in the proximal chamber 66. As the nozzle is withdrawn, the volume of the proximal chamber 66 reduces and the volume of the compressible member 41 increases. This forces liquid from the proximal chamber 66 into the narrow channels 43, and then



out the distal port 50. When the valve 5 returns to the closed mode, the proximal chamber 66 has a minimum volume while the compressible member 41 has a maximum volume. As the valve 5 returns to closed mode, liquid formerly in the proximal region in excess of the minimum proximal chamber volume thus was forced from the proximal chamber 66, into the narrow channels 43, and toward the distal port 50. As can be deduced by those skilled in the art, this creates a positive pressure from the distal port 50, consequently preventing (or substantially reducing) fluid drawback that can cause blood or other contaminants to be drawn into the valve 5.

Instead of the narrow channels 43, liquid may be directed to the distal port 50 by some other means. Accordingly, principles of the invention should not be limited to those embodiments requiring narrow channels 43.

Figure 4 shows a cross-sectional view of a second embodiment of the valve 5 shown in figure 1. In this embodiment, the outlet housing portion 48 is reconfigured to have an orthogonal outlet 100 for directing fluid from the valve 5, and an end cap 102 at its distal end. Further unlike the embodiment shown in figure 1, the compressible member 41 is in the form of a hollow cylinder having a closed top portion, and an open bottom portion (figure 5A). In particular, the top portion comprises a top surface 104 having a depression 106 for receiving the bottom portion of the cannula 14. The bottom portion includes an annular flange 108 for securing the compressible member 41 within the valve 5 (discussed below). The compressible member 41 may be manufactured from any material used in the art, such as silicone, latex, or plastic, that can compress and decompress without significantly affecting its overall structure.

As shown in figure 4, the compressible member 41 is free standing within the chamber 65. Accordingly, when in the closed mode, the side of the compressible member 41 do not directly contact the side walls of the fluid chamber 65. In illustrative embodiments, the side of the compressible member 41 is between about 0.002-0.010 inches from the side walls of the chamber 65. This distance from the interior walls of the chamber 65 provides some additional clearance for compressing the compressible member 41. In other embodiments, there is no such clearance and thus, the compressible member 41 compresses by collapsing upon its interior only.

The compressible member 41 in this embodiment (figure 4) includes a member interior 112 having a conventional spring 114 disposed therein. Although not necessary in many embodiments, the spring 114 may be provided to supply additional proximal biasing force for normally biasing the member 41 in a proximal direction. The spring 114 may be any spring known in the art, such as a coil spring, or an integral piece of material that provides the additional biasing force (figure 6). In other embodiments, the member interior 112 is empty and thus, it has no internal spring 114. In such other embodiments, the compressible member 41 preferably is manufactured from a material and/or with a geometry that normally biases the compressible member 41 proximally. In fact, such embodiments of the compressible member 41 themselves are springs. Additional details of such member geometry are discussed below with reference to figure 7.

As noted above, the valve 5 shown in figures 4 and 6 also differ from that shown in figures 1 in that it includes the outlet that extends from the side of the valve 5. In particular, the chamber 65 includes an interior wall that defines an opening 120 to an outlet channel 122 that is formed through an outlet tube 124. The outlet tube 124 may include an annular skirt 126 having threads 128 for coupling with a complimentary connector device. The outlet tube 124 thus is substantially orthogonal to the longitudinal dimension of the valve 5. In some versions of this embodiment, the compressible member 41 may be positioned in the chamber 65 to normally occlude the outlet, thus preventing fluid flow from the chamber 65.

Further unlike the embodiment shown in figure 1 (as noted above), the second illustrative embodiment of the valve 5 also includes the end cap 102, which is ultrasonically welded to its proximal end. As shown in figures 5B-5D, the end cap 102 includes a top surface that forms a part of the member interior 112. The top surface thus defines three venting grooves 130, an annular protrusion 132 for securing the spring 114 (if any) within the member interior 112, and an annular ridge 134 for mating with a complimentary part of the valve housing for securing the end cap 102 to the valve 5.

The cap 102 preferably is connected to the distal end of the housing so that it defines a small annular space 136 ("cap space 136," or referred to by those skilled in the art as a "reveal")

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between it and the housing. In preferred embodiments, the cap space 136 is between about 0.002 and 0.004 inches. The bottom portion of the compressible member 41 is secured over the three venting grooves 130 to the top surface of the cap 102. Each groove is in fluid communication with the cap space 136 to form a vent 140 that vents the member interior 112 to the exterior of the valve 5. Of course, vents may be interpreted herein to include any channel that extends from the member interior 112 to the exterior of the valve 5. Accordingly, various embodiments of the invention are not to be limited to the specific disclosed vent configurations.

The member interior 112 preferably is fluidly isolated from the rest of the chamber 65 (*i.e.*, the chamber area that is exterior to the compressible member 41). To that end, the outlet housing portion 48 includes a distal rim 144 that, when coupled with the end cap 102, compresses the annular flange 108 around the bottom portion of the compressible member 41 to form a liquid tight pinch-fit seal. This seal ensures that liquid does not leak into the member interior 112. Accordingly, the rim 144 may be flat, or may converge to a pointed annular ring that pinches the member annular flange 108.

When the compressible member 41 is compressed, air within the member chamber (*i.e.*, the chamber formed by the interior of the member 41) is forced out of the member interior 112 through the vents, thus facilitating compression of the compressible member 41. Among other ways, the resistance to compressing the compressible member 41 may be adjusted by adjusting the size and geometry of the vents. Conversely, when the compressible member 41 is decompressed, air from the exterior of the valve 5 is drawn into the member interior 112, thus facilitating decompression of the compressible member 41.

Accordingly, when in the closed mode, the compressible member 41 is fully decompressed, thus causing the proximal chamber 66 to have a minimum volume. When in the open mode, the compressible member 41 is compressed to enlarge the proximal chamber 66 to its maximum volume. Liquid or other fluid injected through the cannula 14 and transverse gland 12 28 thus flows into the proximal chamber 66, and out of the valve 5 through the outlet. To direct fluid to the outlet, this embodiment of the valve 5 may have one or more narrow flow channels (similar to those in the valve 5 of figure 1), or the clearance between the compressible member 41

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and the interior wall of the chamber 65 may form a channel. In yet other versions of this embodiment, the compressible member 41 normally occludes the outlet. Accordingly, to open the valve 5, the compressible member 41 of this version must be forced distally until the top of the compressible member 41 is more distal than the top of the outlet channel 122, thus fluidly communicating the proximal chamber 66 with the outlet.

Figure 7 shows a cross-section of a third illustrative embodiment of the valve 5 shown in figure 1. In a manner similar to that shown in figure 4, this embodiment includes the orthogonal outlet 100, the compressible member 41 with an open distal end, and the vented end cap 102. Unlike the embodiment shown in figure 4, however, the top portion of the compressible member 41 is contoured to a complimentary shape to that of the bottom portion of the cannula 14. For example, as shown in figure 7, both the bottom portion of the cannula 14 and the top portion of the cannula 14 are flat. Each of the embodiments described herein may have a similar complimentary geometry.

In addition, the compressible member 41 also is shaped in a distally bowed configuration to further enhance its proximal biasing force. In particular, the compressible member 41 of this embodiment includes an upper portion 148 having a substantially uniform outer diameter, a diverging middle portion 150 having a distally expanding outer diameter, and a lower portion 152 having a substantially uniform inner diameter. In a manner similar to other embodiments, the lower portion 152 includes the annular flange 108 for securing the compressible member 41 within the complimentary recess of the valve 5. The upper portion 148 includes an inner surface 154 (*i.e.*, defining a portion of the member interior 112) having a substantially uniform radius for providing support for the cannula 14 upon its top portion.

As shown in the figure, this embodiment of the valve 5 does not include a spring with the member interior 112. Although not necessary, one may be provided to further proximally bias the compressible member 41. Some versions of this embodiment may utilize an inverted cone type of compressible member 41 (not shown), where the compressible member 41 has an hourglass shape. Similar to the distally bowed compressible member 41, a compressible member 41 in an

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inverted cone configuration generally readily returns to its normal uncompressed state when distally applied force is not applied to its top portion.

Figure 8 schematically shows a fourth illustrative embodiment of the valve 5 shown in figure 1. In a manner similar to the embodiment shown in figure 1, the distal port is located at the proximal end of the valve 5 and not orthogonal to the flow channel through the cannula 14. Also like the embodiment shown in figures 4, 6, and 7, the compressible member 41 is hollow and open distal ended similar to the embodiment shown in figure 5A. It should be noted that although the compressible member 41 with a substantially uniform outer diameter is shown, various other compressible members may be utilized, such as the compressible member 41 shown in figure 7. Although not shown, some versions of this embodiment include a spring 114 within the member interior 112.

The chamber 65 in the fourth illustrative embodiment forms a vent 155 that extends through the housing, thus venting the member interior 112 to the atmosphere. In addition, this embodiment also includes two distal flow channels 156 that fluidly connect the chamber 65 (*i.e.*, the part of the chamber 65 that is external to the member interior 112) with the distal port 50. Accordingly, when in the open mode, fluid is directed from the proximal chamber 66, through the narrow flow channel(s) 43 in the side of the interior walls to the distal flow channels 156, to the distal port 50. Moreover, when the compressible member 41 is compressed, air is expelled from the member interior 112 via the vent 155. In a similar manner, when the compressible member 41 decompresses, air is drawn into the member interior 112 to facilitate its decompression.

It should be noted that although a swab valve is shown in the disclosed embodiments, other valves may be utilized in accord with the various embodiments disclosed herein. Moreover, in some embodiments implementing a swab valve, the slit top surface of the gland 12 may be substantially flush with the proximal opening to the valve 5 (*e.g.*, see figure 8), while in other embodiments, such surface extends above the proximal opening (*e.g.*, see figure 4).

Although various exemplary embodiments of the invention have been disclosed, it should

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be apparent to those skilled in the art that various changes and modifications can be made which will achieve some of the advantages of the invention without departing from the true scope of the invention. These and other obvious modifications are intended to be covered by the appended claims.

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